## **CLAIMS**

- 1. 52. (CANCELLED)
- 53. (CURRENTLY AMENDED) A method of estimating arterial delay and arterial dispersion (t, α, σ) values for outputting blood perfusion indices for a region of interest (ROI) by from operating a computer program on intensity data [[in]] input to a computer comprising:
- a. using a computer to apply applying a first gamma-variate function (GVF) to an arterial input function (AIF<sub>a</sub>) using a computer to provide an estimated first model of a vascular transport function h<sub>a</sub>(t), wherein for t <</li>
  10 t<sub>1</sub>, h<sub>a</sub>(t) = 0 and for t ≥ t<sub>1</sub>, h<sub>a</sub>(t) = 1/σ<sub>1</sub> (t t<sub>1</sub>)<sup>α<sub>1</sub></sup> e<sup>-(t-t<sub>1</sub>)/σ<sub>1</sub></sup>, wherein t<sub>1</sub> is the transit time of a contrast agent from a measured initial said AIF<sub>a</sub> to a region of interest (ROI) and σ<sub>1</sub> is an estimating estimate of an initial delay dispersion value of said contrast agent, wherein said σ<sub>1</sub>=(t<sub>1</sub>)(β<sub>1</sub>)/(1-β<sub>1</sub>), wherein said β<sub>1</sub> is a known relative dispersion value having a range from 0 to 1;
  - b. using a computer to convolve convolving AIF<sub>a</sub>(t) with said  $h_a(t)$  with  $\alpha_1=0$  using a computer for obtaining an arterial input function AIF<sub>1</sub>(t) = AIF<sub>a</sub>(t)  $\otimes$   $h_a(t)$  with  $\alpha_1=0$  at said ROI;
  - c. using a computer to estimate estimating a blood flow rate  $F_t$  and a tissue impulse residue function  $R_e(t)$  using a computer by deconvolving a concentration curve  $C(t) = (F_t/k_H)AIF_t(t) \otimes R_e(t)$ , wherein  $k_H$  is a hermatocrit hematocrit correction constant having a known value, wherein

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- a tissue transport function  $h_e(t)$  is determined by  $h_e(t) = -dR_e(t)/dt$ ;
- d. using a computer to optimize said mean transit time and dispersion ( $t_2$ ,  $\alpha_2$ ,  $\sigma_2$ ) values using a least squares method from an estimated transport function  $h_e(t)$ ; and
- e. using a computer to output inputting said estimated and optimized calculated tissue mean transit time and dispersion (t<sub>2</sub>, \alpha\_{27}, \sigma\_{2}) values from an estimated transport function h<sub>0</sub>(t) for input to a simulated transport function h<sub>0</sub>(t), wherein a simulated tissue impulse residue function R<sub>0</sub>(t) is determined, wherein a simulated concentration curve C<sub>0</sub>(t) is fitted to said measured C(t) and quantitative said blood perfusion indices are calculated, wherein each said step is performed by a suitably programmed computer.
- d. determining a simulated transport function  $h_s(t) = \frac{1}{A_2} (t t_2)^{\alpha_2} e^{-(t t_2)/\sigma_2}$ when  $t \ge t_2$  and  $h_s(t) = 0$  when  $t < t_2$ , wherein  $A_2 = \sigma_2^{1 + \alpha_2} \Gamma(1 + \alpha_2)$ , wherein said  $h_s(t) = \frac{1}{A_2} t^{\alpha_2} e^{-t/\sigma_2}$  when said  $t_2 = 0$ , or said  $h_s(t) = \frac{1}{\sigma_2} e^{-(t t_2)/\sigma_2}$  when said  $\alpha_2 = 0$ , wherein said  $\alpha_2$  is a dispersion of said  $\alpha_2$  and said  $\alpha_2$  is a mean transit time of said  $\alpha_2$ , wherein when said  $\alpha_2 = 0$  a peak height  $(PH)=1/\sigma_2$  and a mean transit time  $(MTT)=t_2+\sigma_2$  are used to determine said  $\alpha_2$ ;
- e. <u>determining a simulated tissue impulse residual function (IRF)</u>  $R_{s}(t) = 1 \int_{0}^{t} h_{s}(\tau) d\tau, \text{ wherein a simulated contrast agent concentration}$   $\underline{C_{s}(t) \text{ is determined by } C_{s}(t) = (F_{t}/k_{H})AIF_{t}(t) \otimes R_{s}(t); \text{ and}}$

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fitting said simulated  $C_s(t)$  to said C(t) by iteratively minimizing S using a least squares method defined by  $S = \sum_t (C(t) - C_s(t))^2$ , wherein said iteratively minimizing S comprises reducing the number of adjustable parameters, wherein said adjustable parameters are reduced to five by fixing said  $\alpha_1=0$  and said  $t_2=0$ , or by fixing said  $\alpha_1=0$  and said  $\alpha_2=0$ , and wherein said adjustable parameters are further reduced to four by fixing said relative dispersion  $\beta_1=-\alpha_1/(\alpha_1+t_1)$  of said  $\underline{h}_e(t)$  resulting in said  $\alpha_1$  dependent on said  $t_1$ ;

wherein each said step is performed by a suitably programmed computer.

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54. (CURRENTLY AMENDED) The method of claim 53, wherein said intensity data is generated by administering a contrast agent to a body lumen of a body during a dynamic imaging scan, wherein said body lumen comprises an artery or <u>a</u> vein, wherein an image response from said contrast agent is recorded to computer data storage in a computer.

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55. (PREVIOUSLY PRESENTED) The method of claim 53, wherein said C(t) is a temporal concentration of said contrast agent obtained from said intensity data, wherein said intensity data comprises contrast images sequentially acquired from a region in a body, whereby said contrast agent concentration is plotted versus time.

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56. (CURRENTLY AMENDED) The method of claim 53, wherein said AIFa is

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based on a measured early arrival contrast agent peak intensity profile from a feeding blood vessel to said ROI.

- 57. (CURRENTLY AMENDED) The method of claim 53, wherein said AIF<sub>a</sub> is scaled upward according to a venous input function (VIF), wherein said VIF is based on a measured late arrival—contrast agent peak intensity profile from a large-vein draining from said ROI.
- 58. (PREVIOUSLY PRESENTED) The method of claim 53, wherein said estimated transit time t<sub>1</sub> is the transit time of said contrast agent from a measured initial said AIF<sub>a</sub> of said contrast agent C(t) in a body lumen to said ROI, wherein said t<sub>1</sub> is estimated from plots of said AIF<sub>a</sub> versus time and said C(t) versus time.
- 15 59. (PREVIOUSLY PRESENTED) The method of claim 53, wherein said  $h_a(t)$  is calculated using said estimated transit time  $t_1$  and said estimated dispersion value  $\sigma_1$ , wherein  $h_a(t)$  with  $\alpha_1$ =0 is plotted versus time.

## 60. - 65. (CANCELED)

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66. (CURRENTLY AMENDED) The method of claim 53, wherein said AIF<sub>t</sub>(t) is measureable in a small lumen showing a delay relative to said AIF<sub>a</sub>(t), wherein optimized values for said  $\sigma_1$  and said  $t_1$  are determined by fitting said simulated

convolved AIF<sub>t</sub>(t) to said measured AIF<sub>t</sub>(t), wherein said relative dispersion  $\beta_1$  is determined and applied to all other said intensity data of said ROI using said  $\beta_1$ , wherein a more robust fitting process is provided by a reduced number of parameters for optimization.

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67. (CURRENTLY AMENDED) The method of claim 66, wherein when said relative dispersion β<sub>1</sub> is determined, said vascular transport function h<sub>a</sub>(t) is described by a single variable said t<sub>1</sub> with a constant said β<sub>1</sub>, wherein a two-step method is used to determine said delay and said dispersion values comprising:

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a. deriving an initial tissue impulse residue function  $R_0(t)$  by deconvolving  $C(t) = (F_0/k_H)AIF_a(t) \otimes R_0(t)$  using a model-free singular value decomposition (SVD) deconvolution method, wherein said time delay  $t_1$  is determined by a maximum position of said  $R_0(t)$  at  $R_0$   $max(t=t_1)$ ; and

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b. determine said AIF<sub>1</sub>(t) at an input of said ROI using said  $h_a(t)$  with said  $t_1$  and said  $\beta_1$  held constant, wherein said  $\sigma_1$  is determined.

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68. (CURRENTLY AMENDED) The method of claim 67, wherein a value of tissue blood flow  $F_t$  and a corrected impulse residue function  $R_e(t)$  are obtained by deconvolving  $C(t) = (F_t/k_H)AIF_t(t) \otimes R_e(t)$  using said  $\frac{SVD \text{ model-free deconvolution}}{R_e(t)} \text{ method, wherein said perfusion indices}$  are determined from a curve of said  $R_e(t)$ , wherein  $MTT = \int_0^\infty R_e(\tau)d\tau$ ,

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69. (CURRENTLY AMENDED) The method of claim 53, wherein said contrast agent is in a tissue ROI having a tissue mean transit time τ, wherein a tissue impulse residue function is approximated by the relation R(t >τ) = Ee<sup>-k(t-τ)</sup> and R(t≤τ) = 1, wherein E is an extraction fraction of said contrast agent in said tissue, wherein k is a constant clearance rate of said contrast agent diffusing from said tissue having a relation k = E\*F<sub>t</sub>/V<sub>e</sub>, wherein V<sub>e</sub>\_is the volume

fraction of extravascular and extracellular space (EES) in said tissue.

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70. (CURRENTLY AMENDED) The method of claim 69, wherein said tissue impulse residue function R<sub>s</sub>(t) of said simulated concentration curve C<sub>s</sub>(t) is replaced by an average impulse residue function that incorporates said contrast agent leaked out of a blood vessel into said tissue and gradually clearing from said tissue, wherein said simulated concentration curve C<sub>s</sub>(t) is fitted to said measured C(t) and quantitative said blood perfusion indices are calculated, wherein said E and said V<sub>e</sub> are additional parameters optimized with other adjustable parameters using a least squares method.

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